

Quasi-simultaneous acquisition of nine secondary ions with seven detectors on NanoSIMS50L: application to biological samples

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We employed a method of electrostatic peak switching allowing for the quasi-simultaneous measurement of ^{16}O , ^{18}O , C_2H , C_2D , $^{12}\text{C}^{14}\text{N}$, $^{13}\text{C}^{14}\text{N}$, $^{12}\text{C}^{15}\text{N}$, P, and S with the NanoSIMS 50L instrument to derive ratios for D/H, $^{13}\text{C}/^{12}\text{C}$, $^{18}\text{O}/^{16}\text{O}$, and $^{15}\text{N}/^{14}\text{N}$ from biological samples. This approach involves two steps: (i) derivation of the D/H ratio from measurements of C_2D and C_2H and (ii) switching of the voltage on deflection plates located in front of two detectors. The method is reliable and easy to set up compared with the magnetic peak-switching mode usually used to perform this type of analysis. Copyright © 2014 John Wiley & Sons, Ltd.

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Introduction

Multi-isotope imaging mass spectrometry (MIMS) is a quantitative imaging methodology that combines secondary ion mass spectrometry analysis (using the NanoSIMS50 instrument) with the use of stable isotope-tagged tracers to study metabolism.^[1–4] The stable isotopes that we commonly use for biological studies are D, ^{13}C , ^{15}N , and ^{18}O . Providing deuterium as heavy water precursor to *de novo* nucleotide synthesis^[5] was recently introduced as a method for tracking cell division with MIMS at the level of a single cell without having to extract genomic material.^[6] With this rationale, we have developed a methodology to simultaneously track a variety of biochemical pathways using molecules tagged with different stable isotopes, including deuterium.

The simultaneous acquisition of H, D, ^{12}C , ^{13}C , ^{16}O , ^{18}O , $^{12}\text{C}^{14}\text{N}$, and $^{12}\text{C}^{15}\text{N}$ is challenging, both because the instrument is equipped with only seven detectors and because its theoretical mass range is constrained by the radius of the magnetic sector. The usual approach to such an analysis is to switch between different magnetic fields with alternating acquisition planes. This method requires cycling of the magnetic field, which is time consuming and not entirely reliable during what is often a multi-hour acquisition period.

The method proposed here takes advantage of the deflection plate located in front of the detectors to acquire two masses with one detector with a fixed magnetic field.^[7] Combining deflection plate switching with the measurement of the secondary ions C_2H and C_2D to derive the D/H ratio^[8] enabled the quasi-simultaneous measurement of D/H, $^{13}\text{C}/^{12}\text{C}$, $^{18}\text{O}/^{16}\text{O}$, $^{15}\text{N}/^{14}\text{N}$, P, and S in histologic sections of mouse small intestine.

Methods/results

Deflection plate switching

The NanoSIMS50L at NRIMS is equipped with seven electron multipliers (EM) and a large radius (680 mm) magnetic sector. In theory,

this allows for the acquisition of secondary ions within a mass range defined as $M_{\text{max}}/M_{\text{min}} = 21$, where M_{min} is the mass recorded from detector EM1 and M_{max} is the mass recorded from detector EM7.^[9] In practice, we have measured ions ranging from mass 1 to mass 25 using the deflection plates located in front of detectors 1 and 7. The main purpose of the deflection plates is to direct a specific mass line into the detector. This is achieved by scanning a secondary ion beam, which may be composed of several ion species of isobaric masses, in front of the exit slit (ExS) (Fig. 1(a)). The method proposed here takes advantage of the ability to alternate the voltage on these plates, which provides an easy and reliable means of switching between different isobaric mass lines of interest to derive the ratios for D/H, $^{15}\text{N}/^{14}\text{N}$, and $^{13}\text{C}/^{12}\text{C}$ quasi-simultaneously. More specifically, we use the deflection plate to acquire two masses with one detector at a fixed magnetic field. Representative mass spectra for the isobars at masses 25, 26, and 27 (obtained from detectors 3, 4, and 5) are shown in Fig. 1. The five expected isobars are clearly seen at mass 26 (Fig. 1(c)). A change of the voltage on the plate from 10 to 23 V allows the recording of the signal for CN and C_2D , respectively. In a similar manner, we can record ions $^{12}\text{C}^{15}\text{N}$ and $^{13}\text{C}^{14}\text{N}$ by applying a change of voltage from -17 to -6 V.

The quasi-simultaneous acquisition of these isotopes, along with P and S, using electrostatic peak switching is described in

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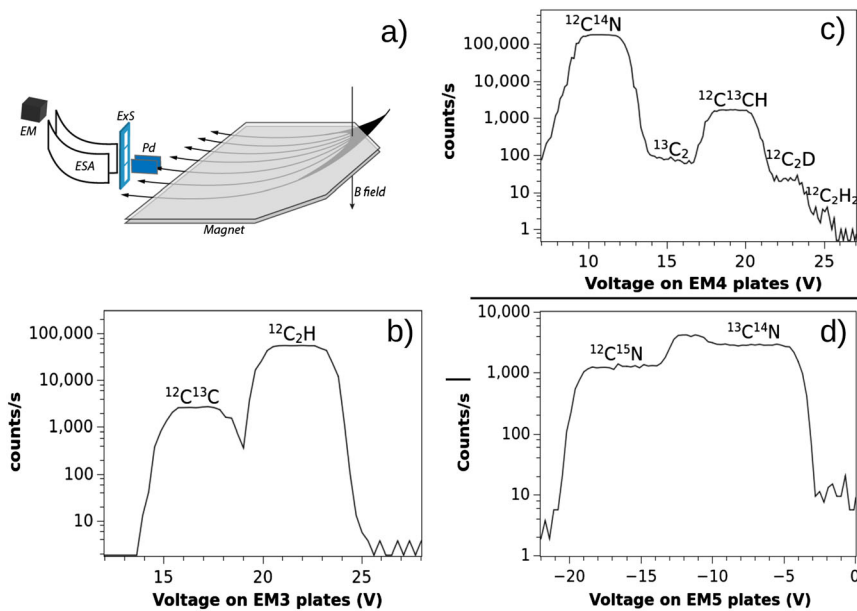


Figure 1. (a) Schematic of the multi-collection on the NanoSIMS50L. The theoretical accessible mass range is $M_{\text{max}}/M_{\text{min}} = 21$ with a 680-mm-radius magnetic sector. Isobaric mass lines are identified by scanning the secondary ion beam of a specific mass in front of the detector's exit slit (ExS) by means of electrostatic plates (Pd). (b–d) High-mass-resolution spectra for the isobars at mass 25, 26, and 27 on detectors EM3, EM4, and EM5, respectively, shown as a function of the voltage applied to the plates (Pd). Mass spectra were obtained from the analysis of a 50- μm field of view on a section of mouse small intestine. The spectrum at mass 26 was obtained with a 20- μm entrance slit (ES4), 150- μm aperture slit (AS3), and a 40- μm exit slit (ExS) at the entrance of detector 4 to adequately resolve C_2D from the other isobaric masses. The mass resolution as defined by Cameca was 12 000 on EM4. For EM5 (d), the spectra are shown for an exit slit (ExS) of 100 μm (9000 MRP).

Table 1. Quasi-simultaneous recording of nine masses with seven detectors on the NanoSIMS50L from three successive scans

Scan	EM1	EM2	EM3	EM4	EM5	EM6	EM7	Ratios measured
1	^{16}O	^{18}O	$^{12}\text{C}_2\text{H}$	$^{12}\text{C}^{14}\text{N}$	$^{12}\text{C}^{15}\text{N}$	^{31}P	^{32}S	$^{15}\text{N}/^{14}\text{N}$ and $^{18}\text{O}/^{16}\text{O}$
2	^{16}O	^{18}O	$^{12}\text{C}_2\text{H}$	$^{12}\text{C}^{14}\text{N}$	$^{13}\text{C}^{14}\text{N}$	^{31}P	^{32}S	$^{13}\text{C}/^{12}\text{C}$ and $^{18}\text{O}/^{16}\text{O}$
3	^{16}O	^{18}O	$^{12}\text{C}_2\text{H}$	$^{12}\text{C}_2\text{D}$	$^{13}\text{C}^{14}\text{N}$	^{31}P	^{32}S	D/H and $^{18}\text{O}/^{16}\text{O}$

Magnetic peak switching function on the Cameca software v 4.1 is used to define the voltage parameters for the plates to apply the method described here.

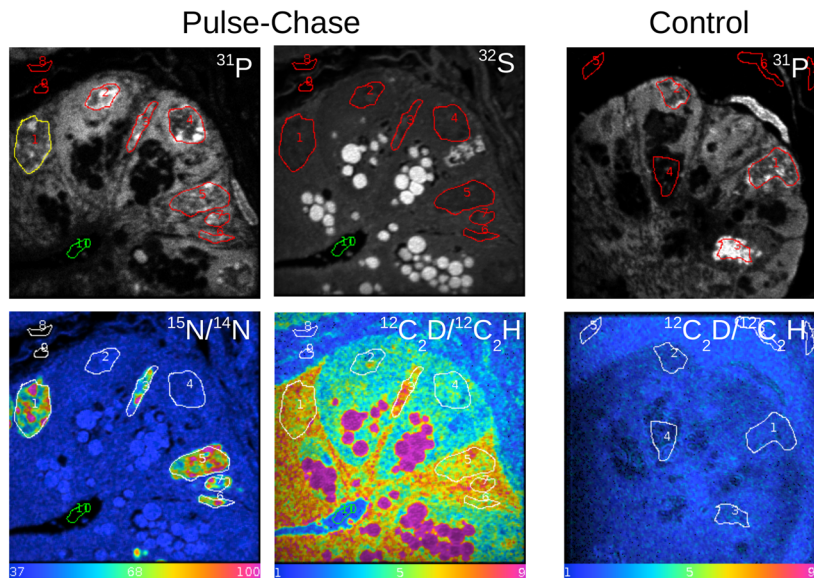


Figure 2. Mouse small intestinal crypt for treated and control mice. Treatment: 8-week-old mice were administered deuterated water ($d_1 = 200 \mu\text{l}$, $d_2\text{--}3 = 30 \mu\text{l}$) and ^{15}N -thymidine ($500 \mu\text{g}$ by intraperitoneal injection) for 3 days (pulse), followed by a 3-day chase period. Field of view is 30 μm , 256×256 pixels. Acquisition time is 131 s/frame for scan 1 (mass 26 on C_2D) and 32 s/frame on scan 2 ($^{12}\text{C}^{14}\text{N}$); 93 planes. Data are processed using the open-source MIMS software.

Table 1. The electrostatic peak switching is operated on EM4 and EM5 to derive the ratios for $^{15}\text{N}/^{14}\text{N}$, $^{13}\text{C}/^{12}\text{C}$, and $\text{C}_2\text{D}/\text{C}_2\text{H}$ from three successive scans. The length of each scan can be set independently. The sequence of three scans can be repeated until a sufficient counting statistic is achieved. The acquisition is quasi-simultaneous in that each scan is of short duration and changes in the sample composition with successive analytical planes is likely trivial in most instances. The method is robust because of the reliability and rapidity in applying different voltages to the plates. It has to be stressed that we did not measure any significant difference in the EM4 detector response to CN or C_2H as controlled from the pulse height distribution. In addition, the useful electrostatic range, defined as deflector plate voltage range where the counting statistic for a given secondary ion is

steady, was determined before each analysis. For EM4, the useful range was [0, +30 V]. For EM5, the useful range was [−30, −10 V], which covers the range required to switch from $^{12}\text{C}^{14}\text{N}$ to C_2D and from $^{12}\text{C}^{15}\text{N}$ to $^{13}\text{C}^{14}\text{N}$.

Application of deflection plate switching to biological sample

We applied this method to analyze sections of LR-white-embedded small intestine from a mouse model. Labeling was achieved by a pulse-chase strategy with deuterated water and ^{15}N -thymidine. We quasi-simultaneously measured the ratios for $^{15}\text{N}/^{14}\text{N}$ and $\text{C}_2\text{D}/\text{C}_2\text{H}$ by applying electrostatic peak switching at mass 26 and 27. The hue saturation image images for $^{15}\text{N}/^{14}\text{N}$ and $\text{C}_2\text{D}/\text{C}_2\text{H}$ are shown in Fig. 2. Regions of ^{15}N -thymidine labeling are observable in the nuclei of divided cells in the crypt of the small intestine in a pattern consistent with chromatin. The $\text{C}_2\text{D}/\text{C}_2\text{H}$ image shows dramatically differential labeling, with extremely high levels of labeling in the sulfur-rich granules contained in Paneth cells. In addition, both the cytoplasm and the nuclei of ^{15}N -thymidine-labeled cells was higher than quiescent (^{15}N -negative) cells. Importantly, this dramatic organelle specific D-labeling pattern cannot be attributable to measurement artifact because of a contribution from the tail of the $^{12}\text{C}^{13}\text{CH}$ peak to the C_2D signal, as measurements taken from an unlabeled intestinal sample (control) did not show a similar differential signal (Table 2).

An important question raised by this methodology is how the intensity of the C_2H ion signal relates to the signals for CH and H from which the D/H ratio can also be derived. Figure 3 shows ion images of a crypt of the small intestine for H, CH, and C_2H ,

Control		
ROI	$^{15}\text{N}/^{14}\text{N}$	$\text{C}_2\text{D}/\text{C}_2\text{H}$
LR-White	38.2 ± 0.12	2.07 ± 0.03
Nucleus	38.1 ± 0.17	2.14 ± 0.03
Cytoplasm	37.9 ± 0.2	2.07 ± 0.1
Granules	38.3 ± 0.15	2.14 ± 0.05

The values reported are the mean and the standard errors on the means for the ratios derived from three ROIs for each category.

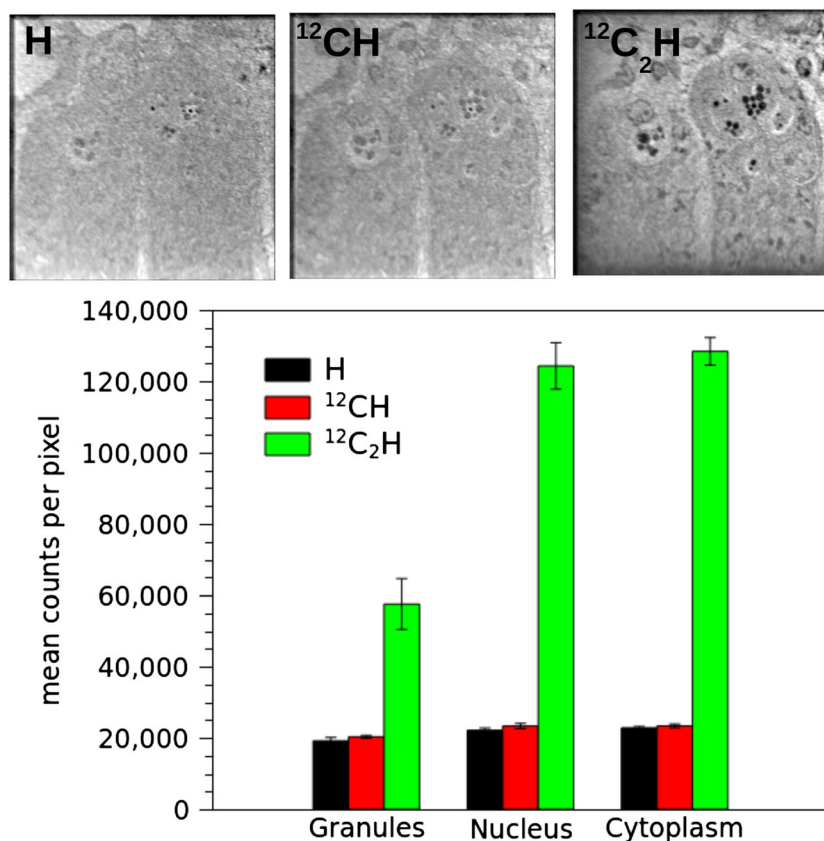


Figure 3. Summed images for H, CH, and C_2H acquired simultaneously. The setup for the mass spectrometer was E53 to correctly resolve the isobars at mass 13 and 25. Image field is $45\ \mu\text{m}$, 256×256 pixels. Acquisition time is 131 s/frame; 160 planes. The histogram shows the counting statistic for H, CH, and C_2H for organelles (nucleus, granules, and cytoplasm) from Paneth cells.

respectively, which were measured simultaneously for purpose of comparison. The C_2H image shows much more contrast than the H or CH images. Moreover, the signal intensity for C_2H is three to eight times higher than that of H and CH, likely due to the high electron affinity (3.4 eV) of this ion.

A small intestinal section taken from a mouse administered deuterated water was analyzed, and D/H and C_2D/C_2H ratio measurements were recorded from the same field consecutively. The two methods yielded an identical ratio measurement averaged over the analytical field ($D/H = 3.137 \pm 1.116$ SD vs $C_2D/C_2H = 3.138 \pm 1.471$ SD, $p = n.s.$).

Conclusion

Using a strategy of deflection plate switching, we demonstrate the feasibility of quasi-simultaneous measurement of ^{16}O , ^{18}O , C_2H , C_2D , $^{12}C^{14}N$, $^{13}C^{14}N$, $^{12}C^{15}N$, P, and S. This approach allows to calculate the D/H ratio from measurements of C_2D and C_2H ions. It enables the near-simultaneous measurements of four isotope ratios from the same sample field. It is of broad applicability in MIMS biological experiments.

Acknowledgements

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